

Deep Inpainting for Photon-Counting Cone-Beam CT

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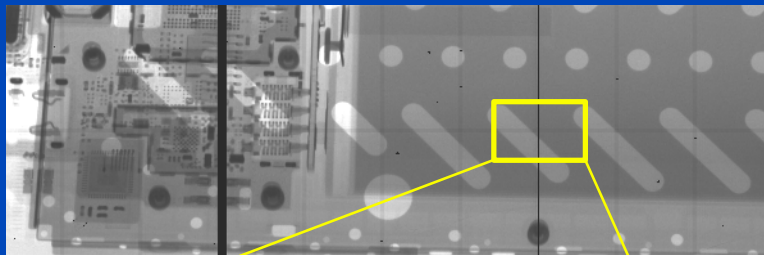
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Motivation

- Photon counting detector technology has proven promising image quality for clinical CT¹.
- Likely that the same holds for CBCT



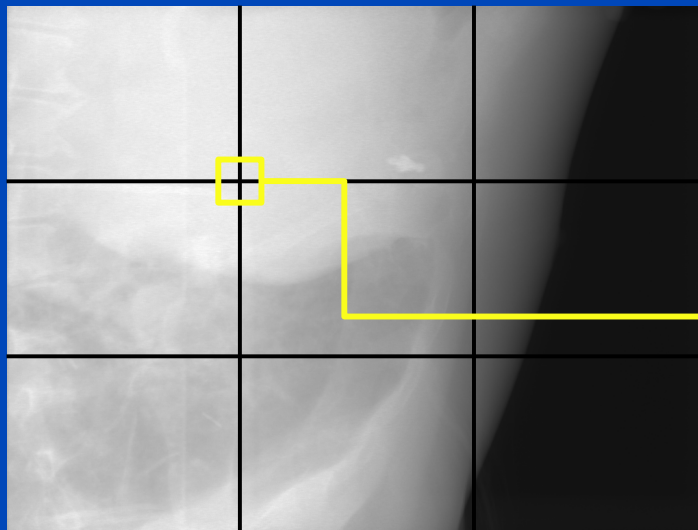
Projection of smartphone from a Dectris Pilatus 3 photon counting sensor

- ASIC modules are limited in size and thus need to be tiled in order to assemble larger flat detectors.
- Several-pixel wide gaps between the modules may occur.
- Need to be inpainted prior to reconstruction or examination of x-ray radiographs or fluoroscopy.

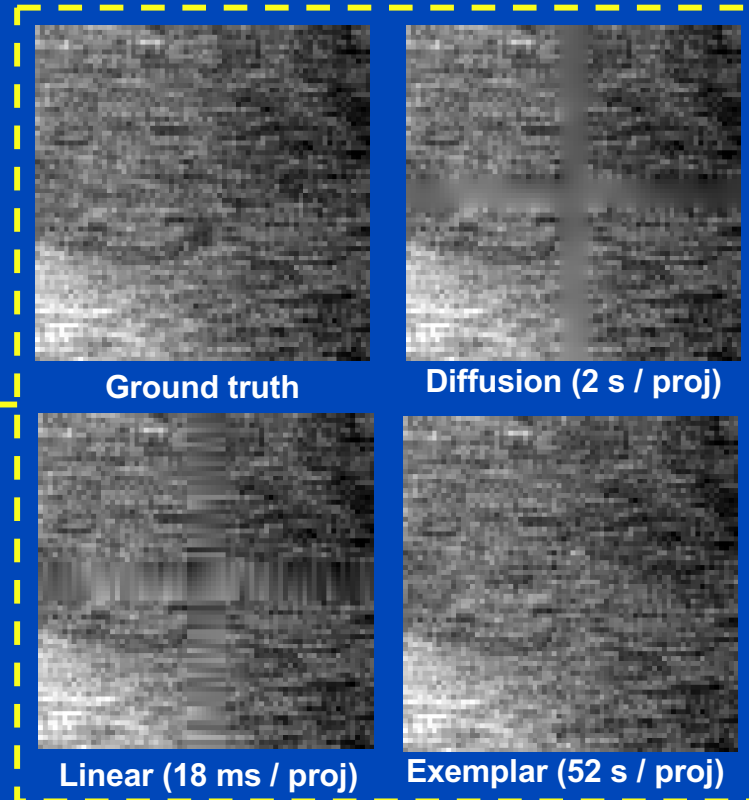
¹ Pourmorteza, Amir, et al. "Abdominal imaging with contrast-enhanced photon-counting CT: first human experience." *Radiology* 279.1 (2016): 239-245.

Prior Work

Existing methods either suffer from inferior quality or long computation times



Single projection (1024×768) from conventional CBCT with artificially induced 6-pixel wide gaps



Methods

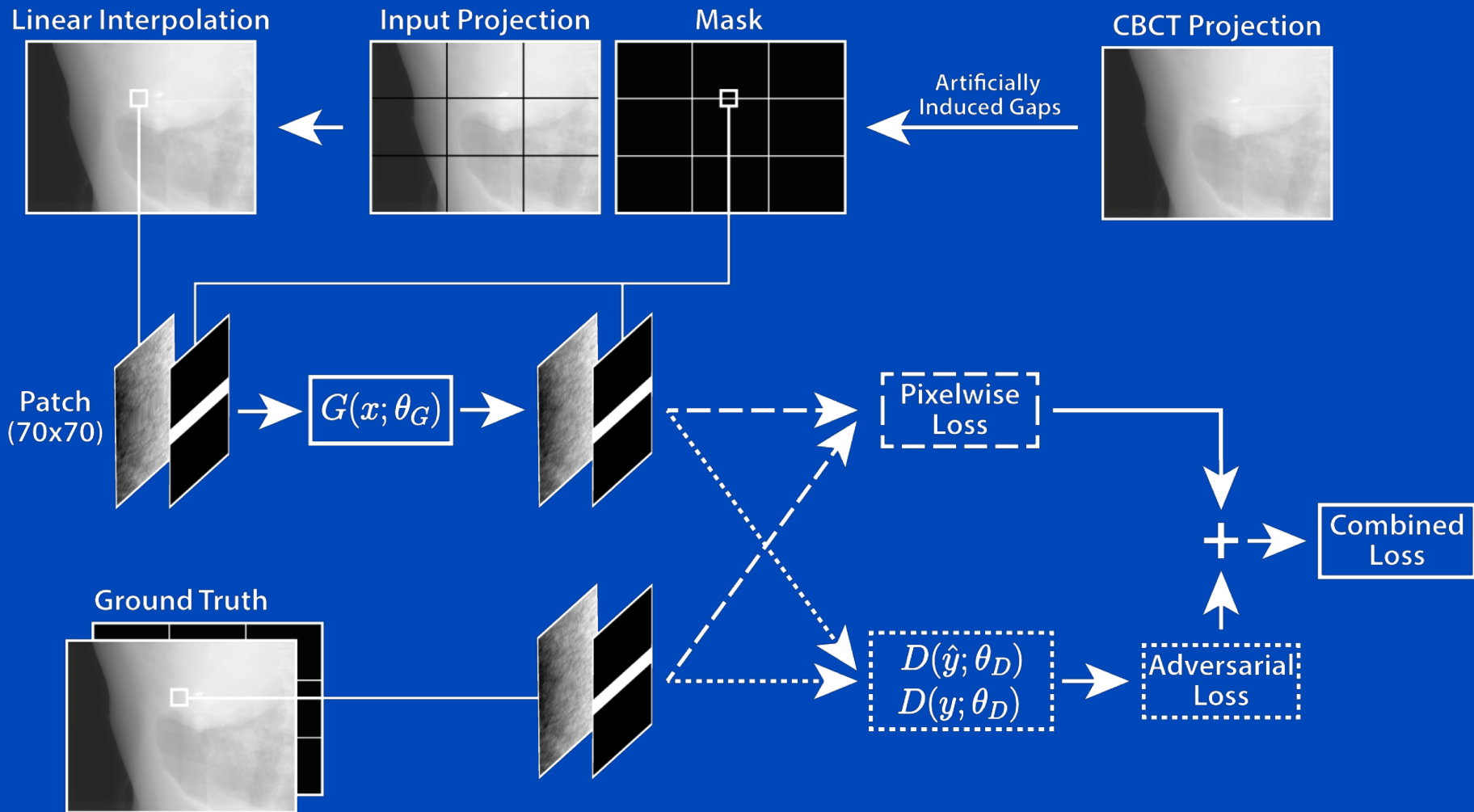
Adversarial Networks for Inpainting

Train adversarial network consisting of Generator G and Discriminator D to fill the dead pixels



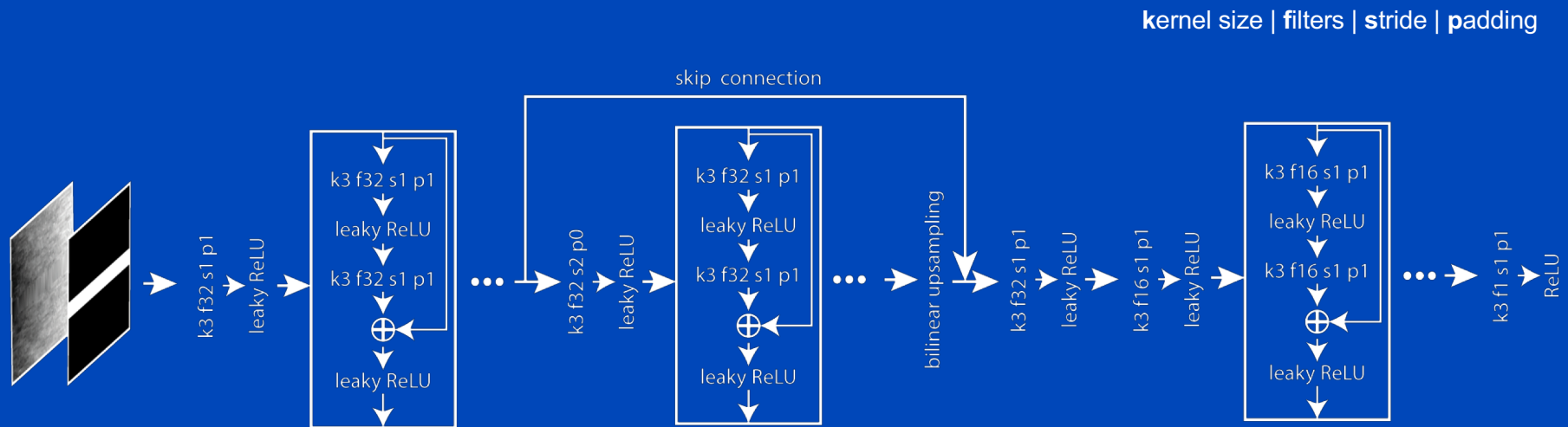
Methods

Training Procedure



Methods

Generator Structure



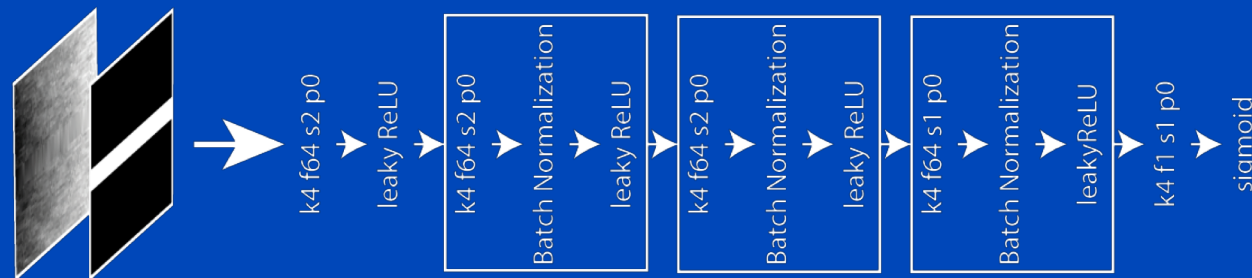
- **Receives patch and mask as input**
- **Fully convolutional**
- **Leaky ReLUs as nonlinearities to further training stability**
- **Consists of several residual blocks¹**
- **One downsampling with skip connection to upsampled image to increase the receptive field.**

¹ He, K., Zhang, X., Ren, S., & Sun, J. (2016). Deep residual learning for image recognition. In Proceedings of the IEEE conference on computer vision and pattern recognition (pp. 770-778).

Methods

Discriminator Structure

kernel size | filters | stride | padding



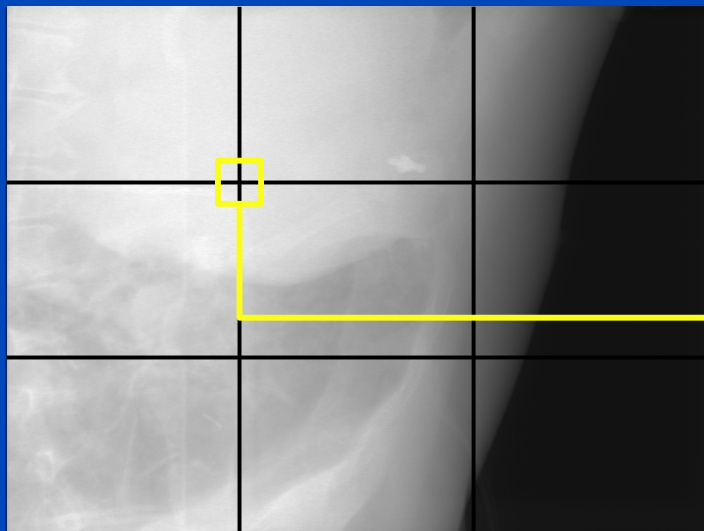
- Receives patch and mask as input
- Fully convolutional
- Leaky ReLUs as nonlinearities to further training stability
- Final nonlinearity is sigmoid to give rating between 0 and 1 whether seen patch originates from ground truth distribution or was generated.

Methods

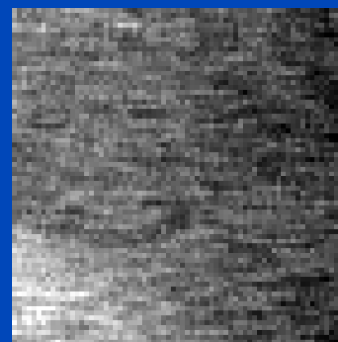
Dataset Details

- **Training**
1 abdomen, 4 thorax CBCT datasets, yielding 3286 projections
- **Validation**
1 abdomen, 1 thorax CBCT datasets, yielding 1314 projections
- **Tube voltage: 125 kV**
- **Scanner: Varian TrueBeam[®]**
- **Detector: Varian 4030 flat detector (40×30 cm)**

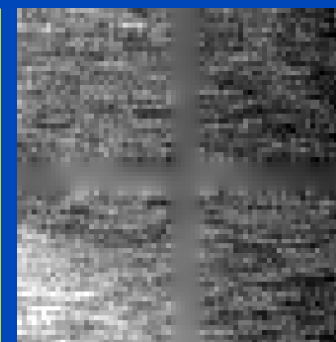
Results



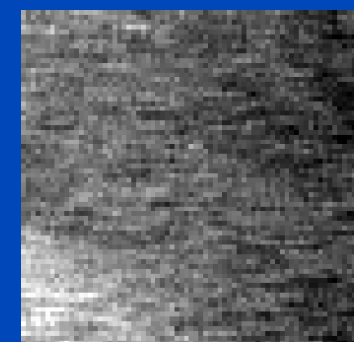
Single projection (1024×768) from conventional CBCT with artificially induced 6-pixel wide gaps



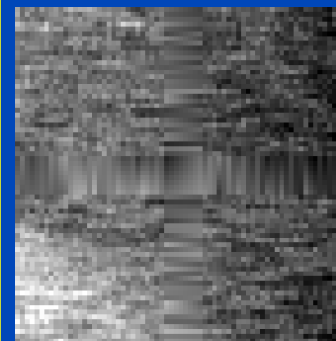
Ground truth



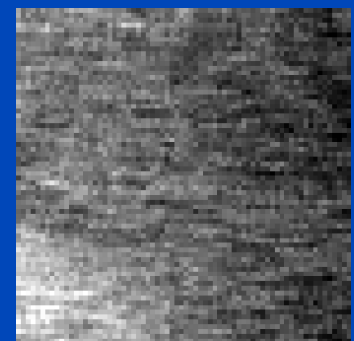
Diffusion (2 s / proj)



Exemplar (52 s / proj)



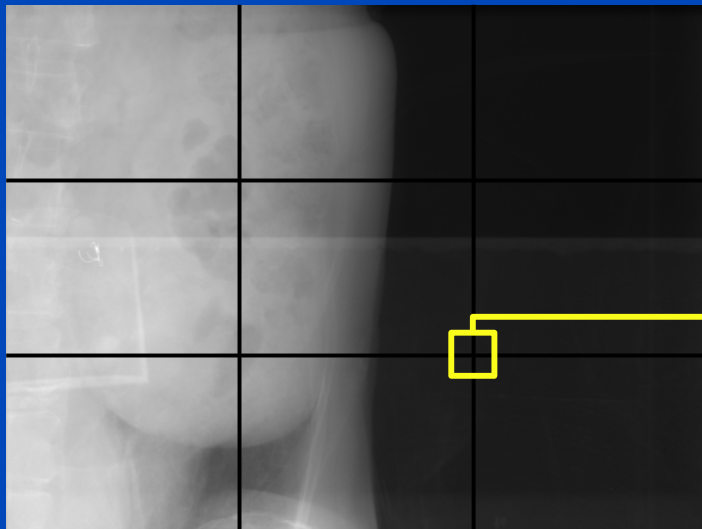
Linear (18 ms / proj)



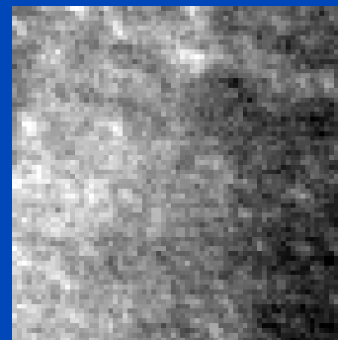
CNN (48 ms / proj)

→ CNN is factor 1000 faster than exemplar-based inpainting

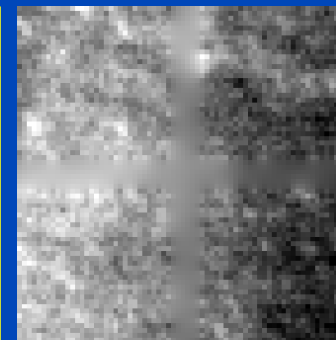
Results



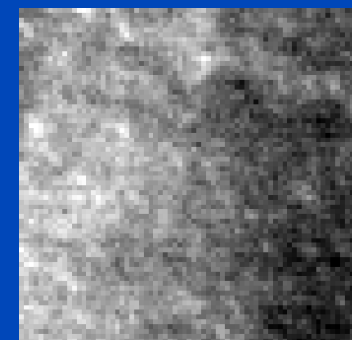
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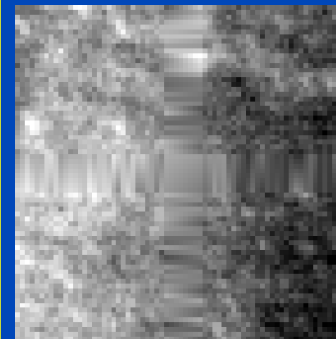
Ground truth



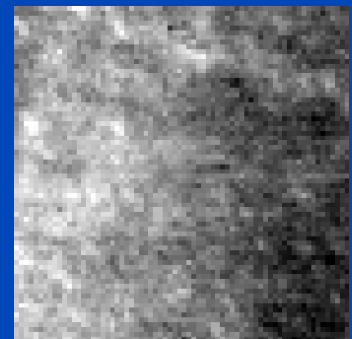
Diffusion (2 s / proj)



Exemplar (52 s / proj)



Linear (18 ms / proj)



CNN (48 ms / proj)

→ CNN is factor 1000 faster than exemplar-based inpainting

Conclusion & Outlook

- Deep inpainting can remove gaps between detector modules as good as exemplar-based inpainting while reducing the computation time by a factor of 1000.
- Proof of principle on data from conventional CBCT
- Deep inpainting does not need gapless data for training. It is rather trained using the data with pixel gaps and dead pixels.
- Brings photon counting detector technology for CBCT one step closer to clinical routine.

Thank You!



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Conference Chair: **Marc Kachelrieß**, German Cancer Research Center (DKFZ), Heidelberg, Germany

This presentation will soon be available at www.dkfz.de/ct.
Job opportunities through DKFZ's international Fellowship programs (marc.kachelriess@dkfz.de).
Parts of the reconstruction software were provided by RayConStruct[®] GmbH, Nürnberg, Germany.