

Dedicated Imaging of the Breast with a Clinical Photon-Counting CT System: A Phantom Study

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Motivation and Aim

- Modern clinical photon-counting CT (**PCCT**) systems provide a spatial resolution that is much higher compared to previous generations of systems.
- This high spatial resolution might allow for the development of applications that were previously restricted to other modalities.
- We want to **investigate** from a physics point-of-view if such a system, the SOMATOM **Naeotom Alpha** (Siemens Healthineers, Germany), allows for **breast imaging**.
- We further aim at **comparing** the result to a dedicated cone-beam breast CT (**BCT**) system (Koning Corp., USA).

Diagnostic PCCT Systems

(as of November 2022)

	Sensor material	Detector pixel size at iso	FOM	Bins	FDA	Pubs	Installations
Canon	CdZnTe	?	50 cm	5	no	?	1 prototype (Japan)
GE	Si, edge on	?	?	?	no	?	2 experimental setups (Sweden, USA)
Philips	CdZnTe	275 × 275 μm	50 cm	5	no	≈22	1 experimental setup (France)
Siemens CounT	GOS/CdTe (dual source)	700 × 600 μm / 250 × 250 μm	50 / 27.5 cm	4	no	≈50	3 experimental systems (Germany, USA)
Siemens CounT+	CdTe	150 × 176 μm	50 cm	4	no	≈11	3 prototypes (Czech Republic, Sweden, USA)
Siemens Alpha	CdTe/CdTe (dual source)	2· 150 × 176 μm	50 / 36 cm	4	Yes	≈40	About 100 worldwide

The additional factor 2 in the detector pixel size column indicates that some scan modes may use binning.

Imaging Systems

Dedicated Breast CT¹ (BCT)



Photon-Counting CT (PCCT)



¹<https://www.auntminnie.com/index.aspx?sec=ser&sub=def&pag=dis&ItemID=110055>

Detector Pixel BCT¹, EICT, PCCT²

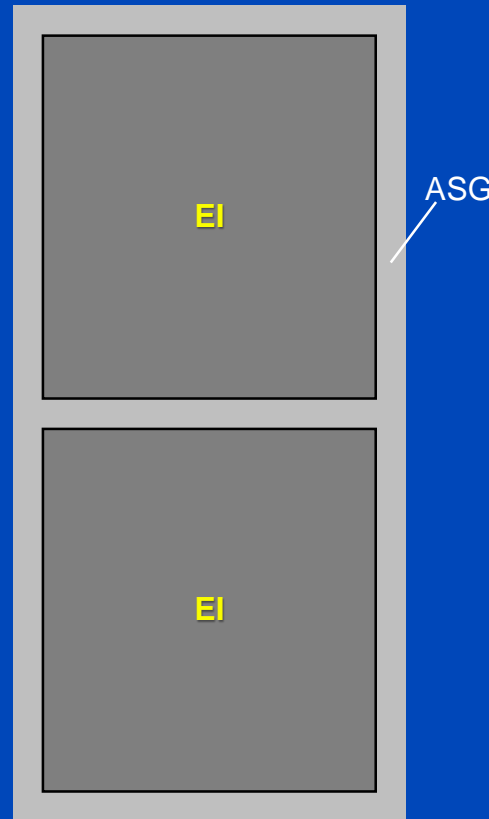
BCT¹

2048 × 1536 pixels
 pixel size 0.273 × 0.273 mm at iso
 209 mm z-coverage



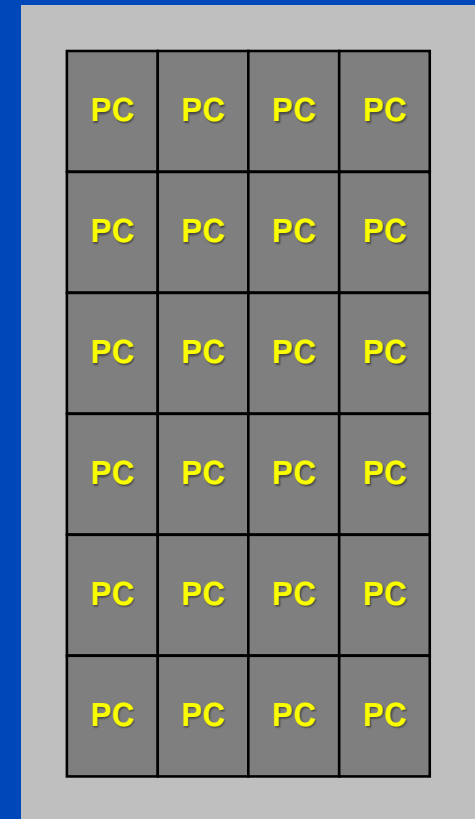
Force

920 × 96 detector pixels
 pixel size 0.52 × 0.56 mm at iso
 57.6 mm z-coverage



Alpha (UHR)²

2752 × 120 pixels
 pixel size 0.15 × 0.176 mm at iso
 24 mm z-coverage



Focus sizes of Vectron tube:
 0.4×0.5 mm, 0.6×0.7 mm, 0.8×1.1 mm

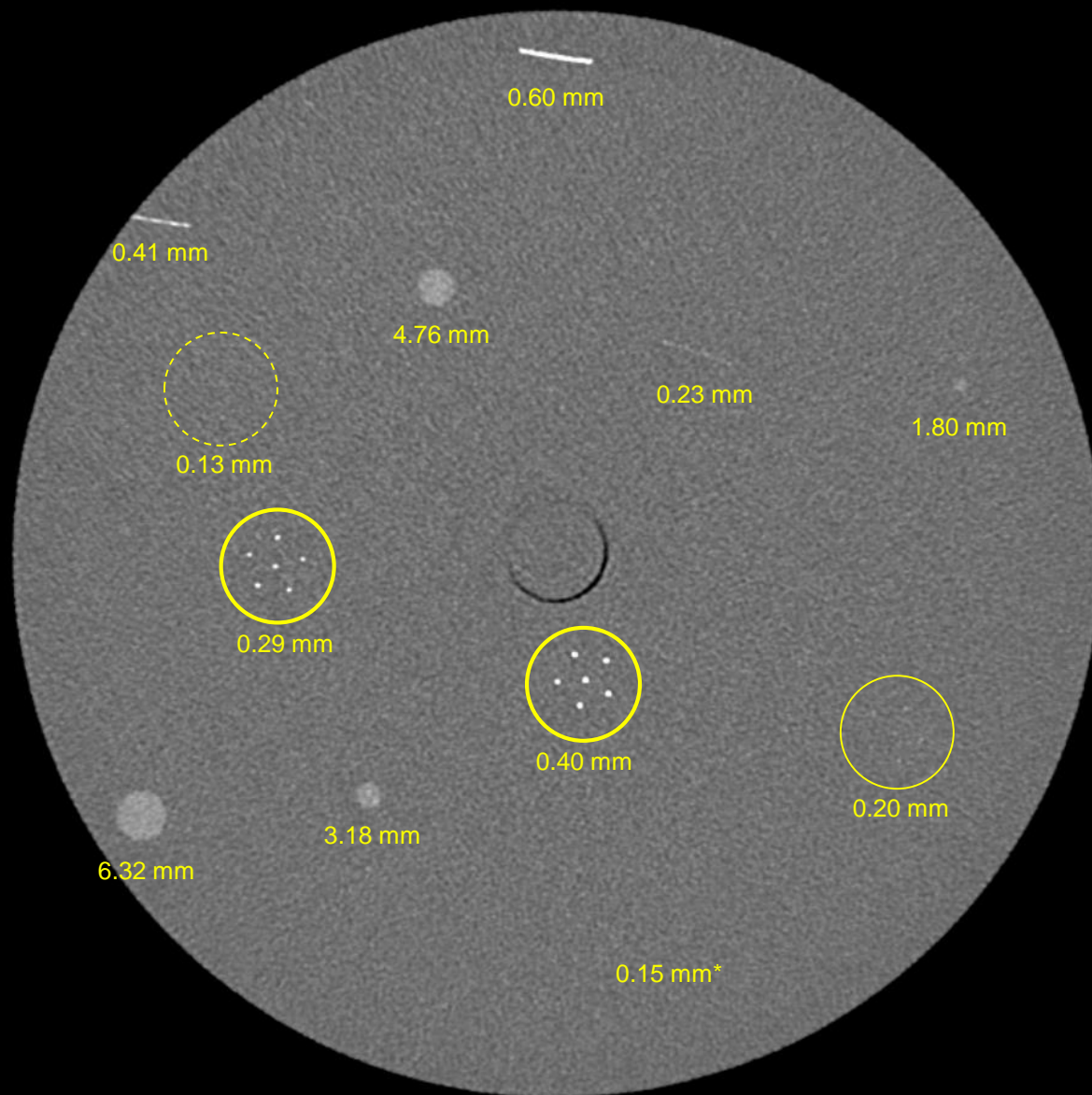
¹L. Brombal et al. Image quality comparison between a phase-contrast synchrotron radiation breast CT and a clinical breast CT: a phantom based study. Scientific Reports 9(1):17778, 2019.

²J. Ferda et al. Computed tomography with a full FOV photon-counting detector in a clinical setting, the first experience. European Journal of Radiology 137:109614, 2021.

Breast Phantom

- 14 slabs of adipose tissue-equivalent material
- Structures of interest:
 - Calcifications
 - Fibers
 - Masses





*barely visible only when scrolling through slices and knowing where to look

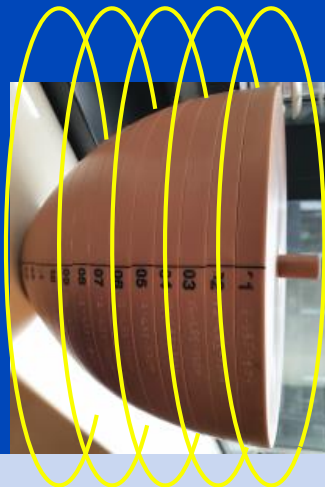
Phantom Orientation

- In case of the dedicated BCT system, the breast phantom can be imaged by itself.
- In case of the PCCT, two phantom positions are used:
 - The phantom is placed on the table and oriented in **longitudinal direction**. I.e., the trajectory of the source is similar to the BCT.
 - The breast phantom is combined **with a thorax phantom** to simulate an actual patient in the clinical scanner.

BCT
(circle)



PCCT
(breast only, spiral)



PCCT
(breast+thorax, spiral)



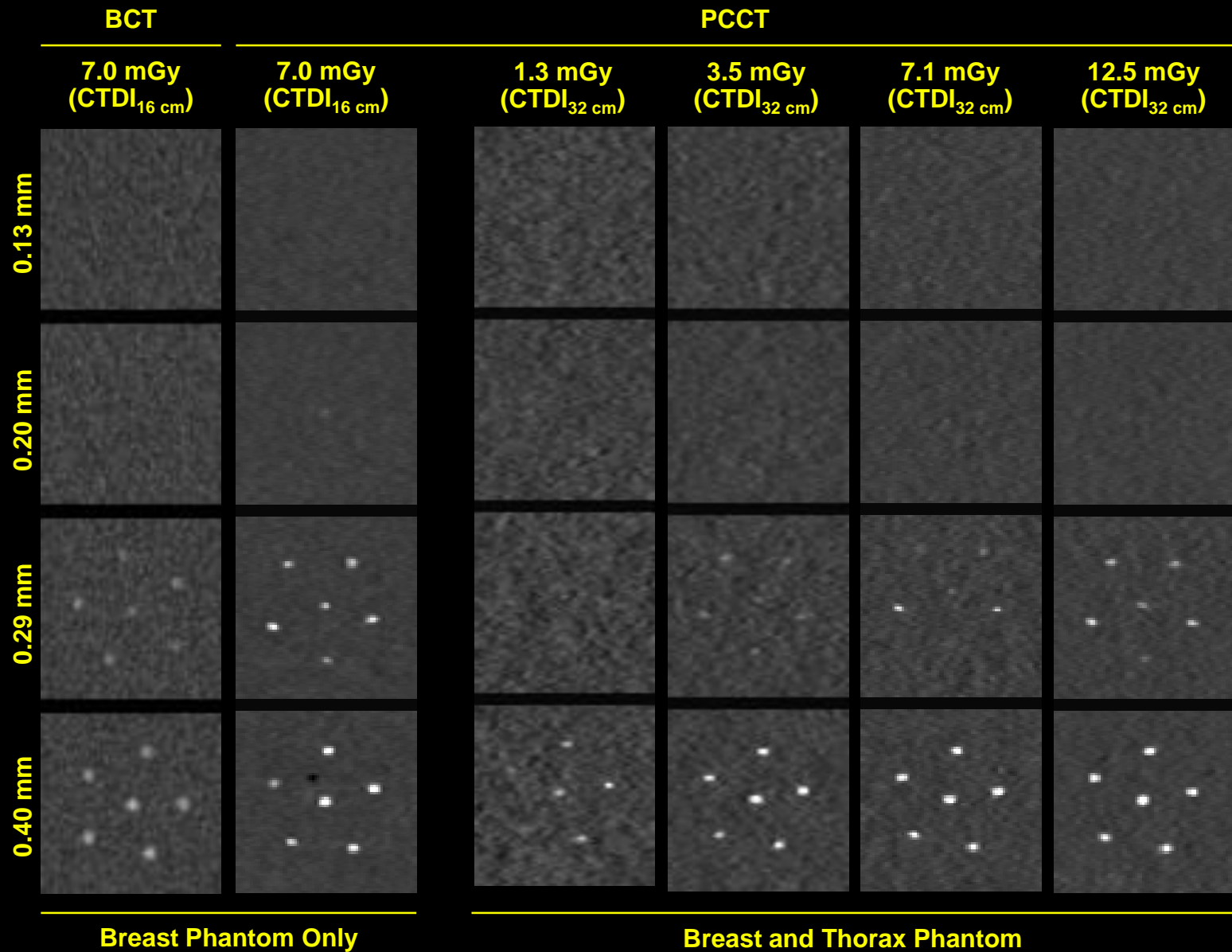
Acquisition and Reconstruction

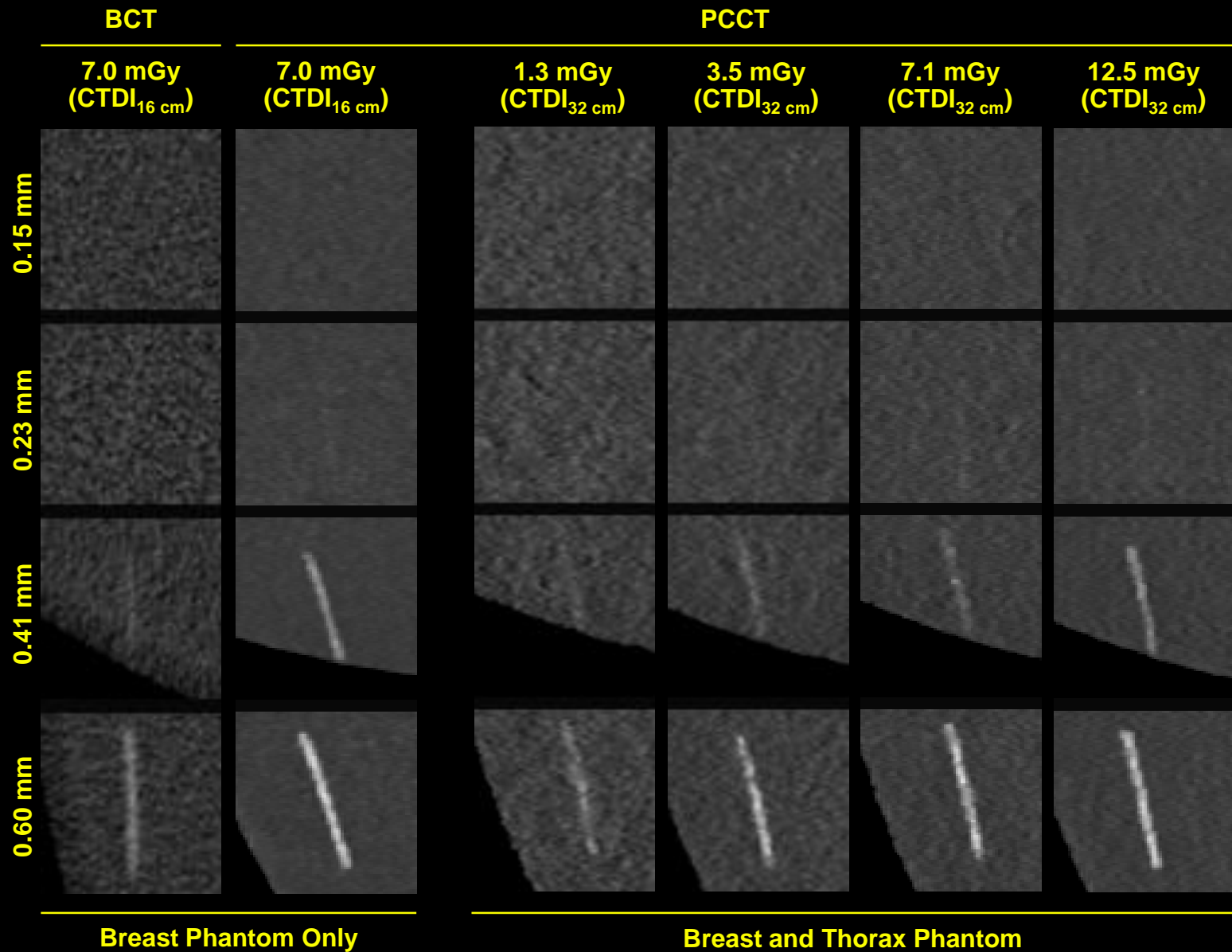
- **BCT:**

- Images using the BCT system were acquired using a tube current of **50 mA** and a tube voltage of **49 kV**.
- BCT data were reconstructed onto a grid of 960×1008 isotropic voxels with a size of 0.19 mm using the **FDK**.


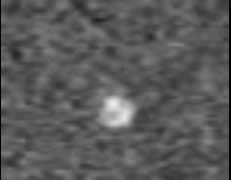
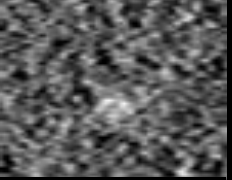
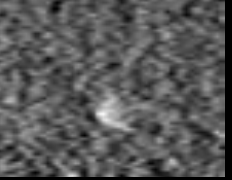
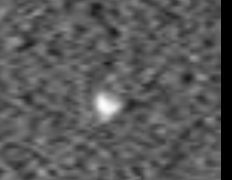
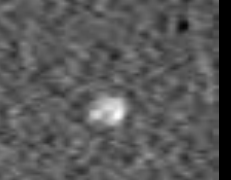

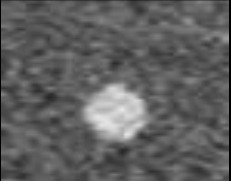

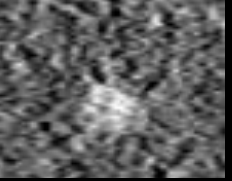
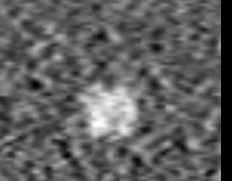
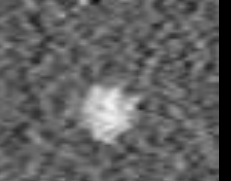
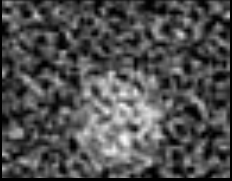
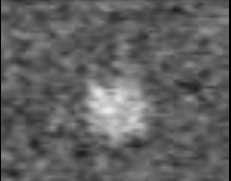
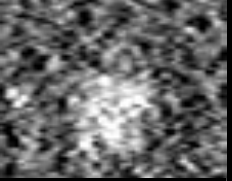
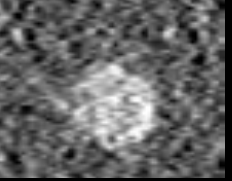
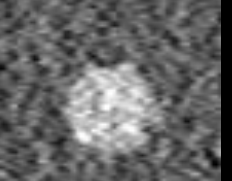
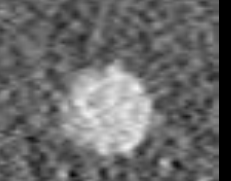


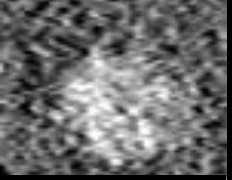

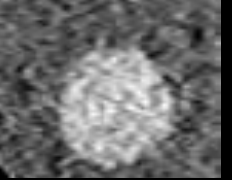
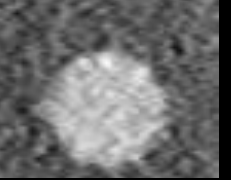
- **PCCT:**

- Images using the PCCT were acquired in UHR mode using tube currents of **41 mA to 350 mA**, respectively, and a tube voltage of **120 kV**.
- No dose modulation was used in any of the experiments.
- Photon-counting data were reconstructed onto slices with 1024×1024 voxels with a size of 0.195 mm, a slice thickness of 0.3 mm and a slice increment of 0.15 mm.
- All data were reconstructed using a B72u-kernel.
- Image reconstruction was performed using Quantum Iterative Reconstruction (**QIR**), strength 3.





0.6 mm MIP, C = 300 HU, W = 1500 HU

	BCT		PCCT			
	7.0 mGy (CTDI _{16 cm})	7.0 mGy (CTDI _{16 cm})	1.3 mGy (CTDI _{32 cm})	3.5 mGy (CTDI _{32 cm})	7.1 mGy (CTDI _{32 cm})	12.5 mGy (CTDI _{32 cm})
1.80 mm	 CNR=1.14	 CNR=4.91	 CNR=1.62	 CNR=2.10	 CNR=3.35	 CNR=3.51
3.18 mm	 CNR=1.26	 CNR=5.47	 CNR=2.12	 CNR=2.25	 CNR=3.34	 CNR=3.37
4.76 mm	 CNR=1.46	 CNR=4.34	 CNR=1.42	 CNR=2.18	 CNR=2.79	 CNR=4.09
6.32 mm	 CNR=2.11	 CNR=4.24	 CNR=1.49	 CNR=2.32	 CNR=2.58	 CNR=3.99
	Breast Phantom Only		Breast and Thorax Phantom			

Summary & Conclusions

- If only the breast phantom is imaged, the BCT and the PCCT show comparable image quality.
- In particular, the CNR in case of the PCCT is better.
- If the breast phantom is combined with the thorax phantom, the PCCT allows for the identification of fibers similar to BCT.
- It also allows for the identification of the larger calcifications.
- Clinical photon-counting CT might be an interesting modality for breast imaging in the future.
- Dedicated scan modes and reconstruction algorithms might further improve image quality.

Thank You!

This presentation will soon be available at www.dkfz.de/ct.
Job opportunities through DKFZ's international Fellowship programs (marc.kachelriess@dkfz.de).
Parts of the reconstruction software were provided by RayConStruct® GmbH, Nürnberg, Germany.